

IEEE Ultrasonic symposium 2002



Short Course 6: Flow Measurements

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Internet-site for short course:

<http://www.ifbt.ntnu.no/~hanst/flowmeas02/index.html>

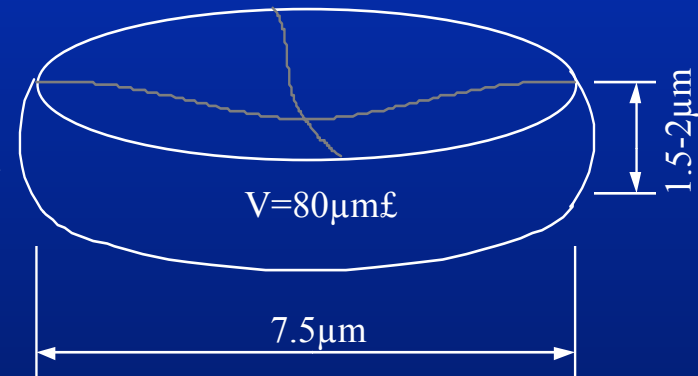
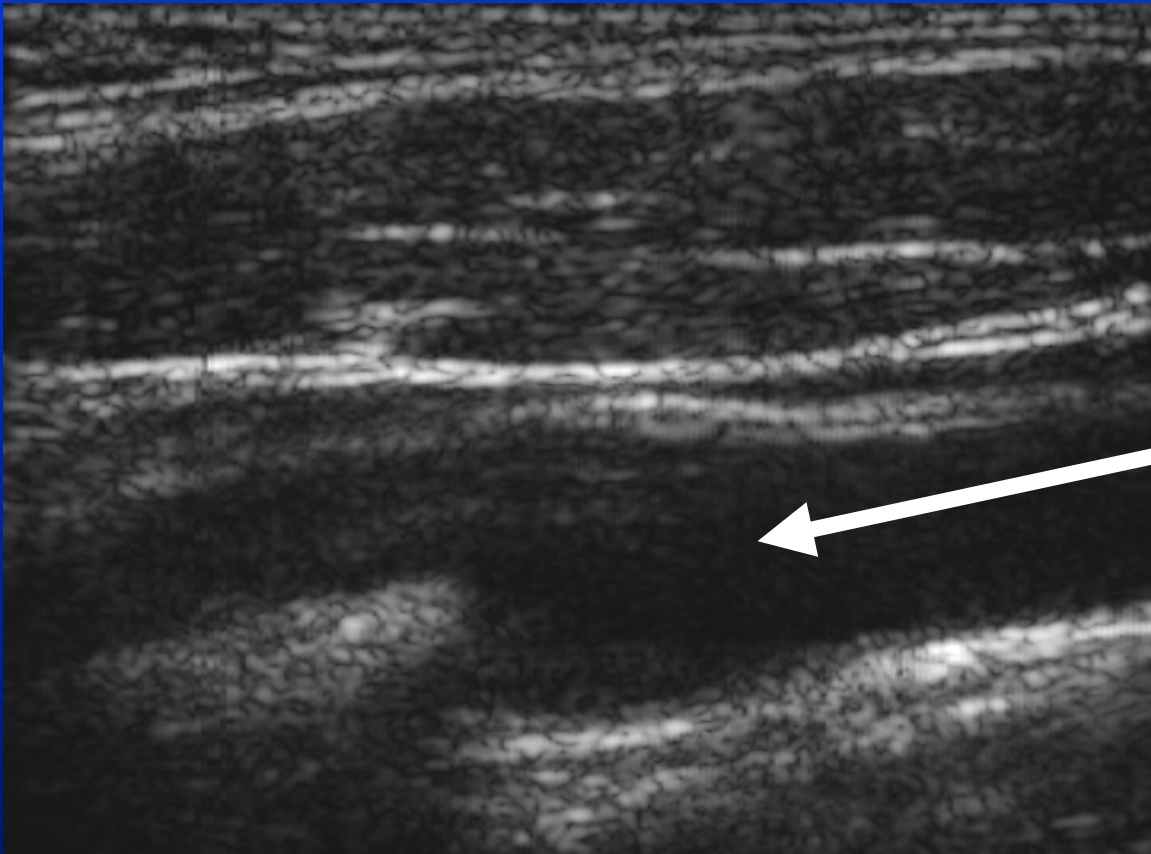
Lecture 1: Introduction

Flow measurements

Introduction

- Course overview. Browsing the [website](#)
- Doppler Techniques for blood flow measurements
- Flow versus velocity measurements. Non-Doppler methods
- Examples on clinical applications

Red blood cells are hardly visible in the ultrasound image

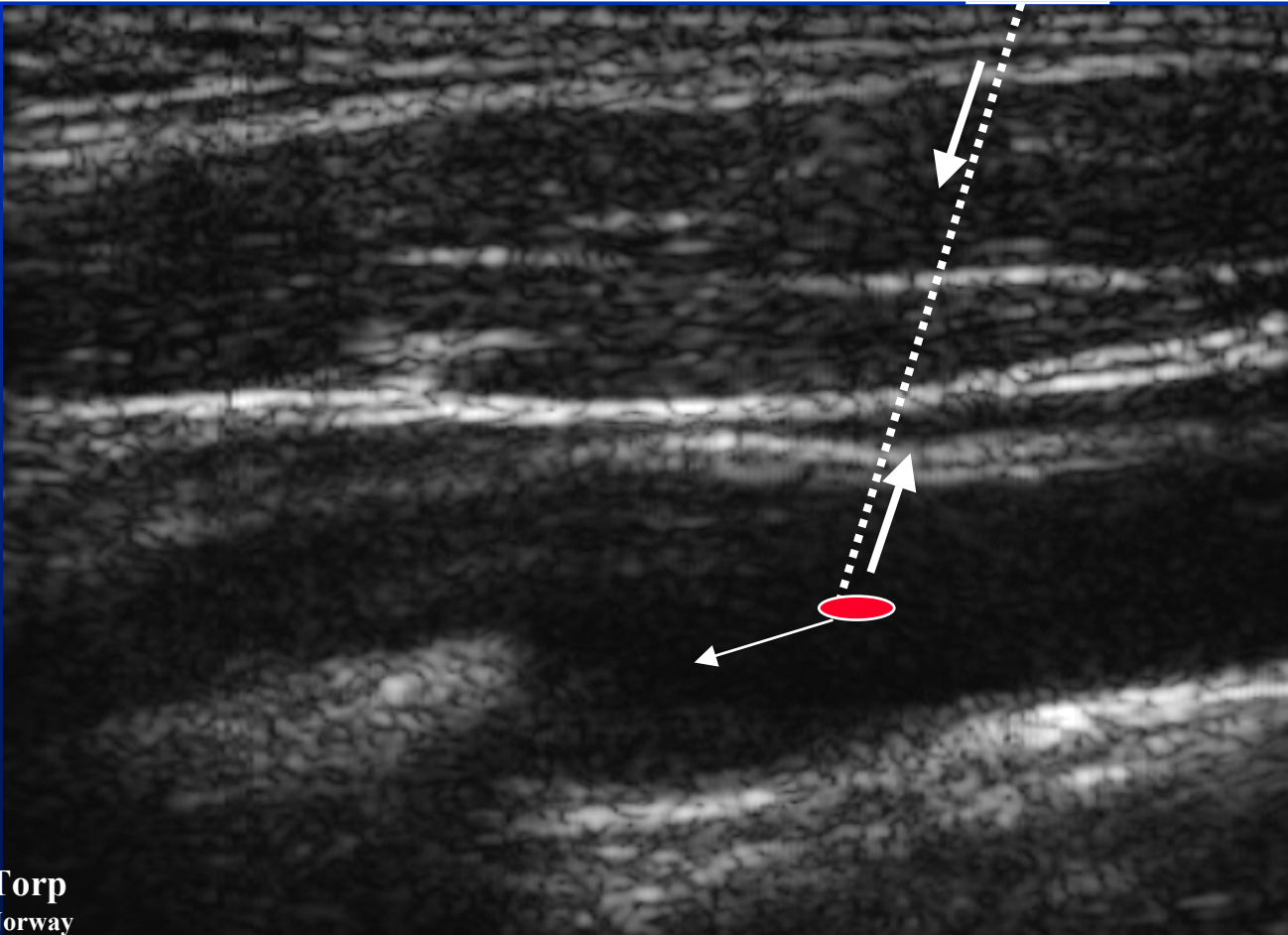


Red blood cell



Ultrasound Doppler

Ultralyd probe



Velocity between sound source and observer gives Doppler shift



Example:

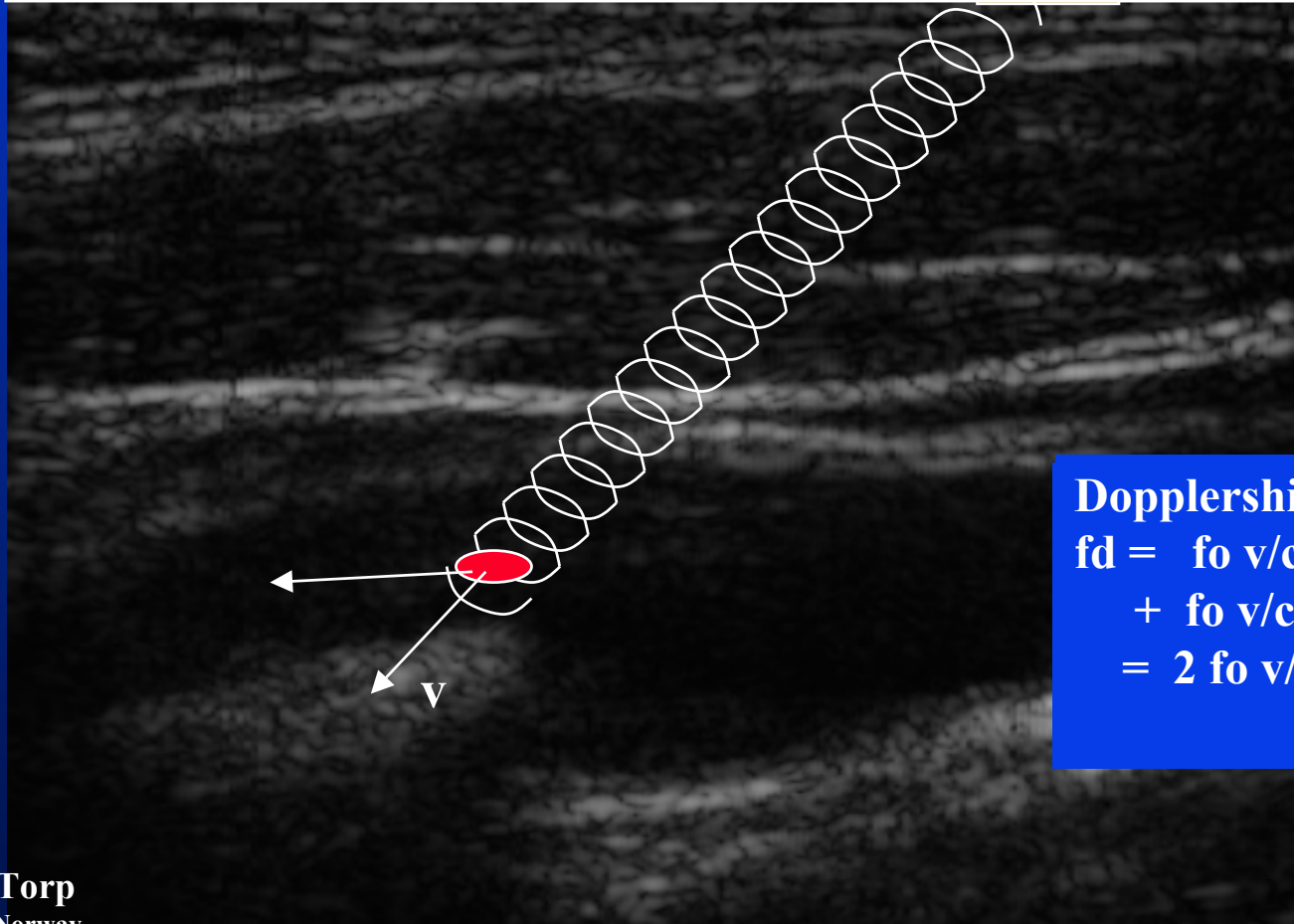
Car speed: 70 km/h \sim 6% of c (speed of sound 340 m/s)

Reduction in pitch: 12 % \sim 2 half tone-interval



Ultrasound Doppler

Ultralyd probe



Dopplershift

$$\begin{aligned} f_d &= f_o v/c \\ &+ f_o v/c \\ &= 2 f_o v/c \end{aligned}$$



Doppler-equation for echoes from moving blood

$$f_d = 2 f_o v \cos(\theta) / c$$

f_d : Dopplershift

f_o : Transmitted frequency

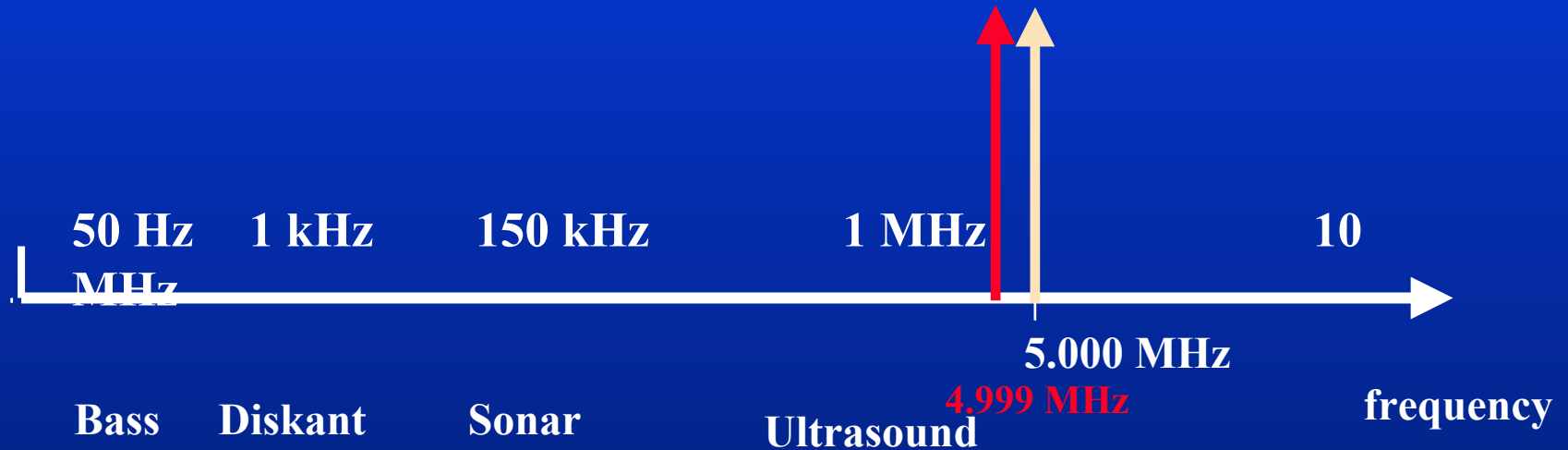
v : Scatterer velocity

c : Speed of sound (1540 m/s)

θ : Angle between v and ultrasound beam



Doppler shift = change in frequency

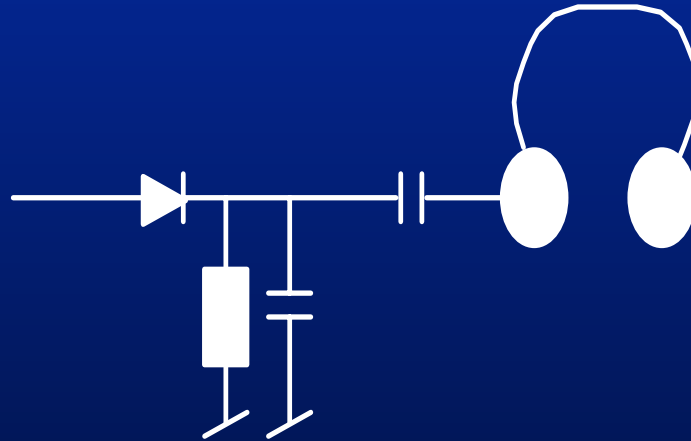
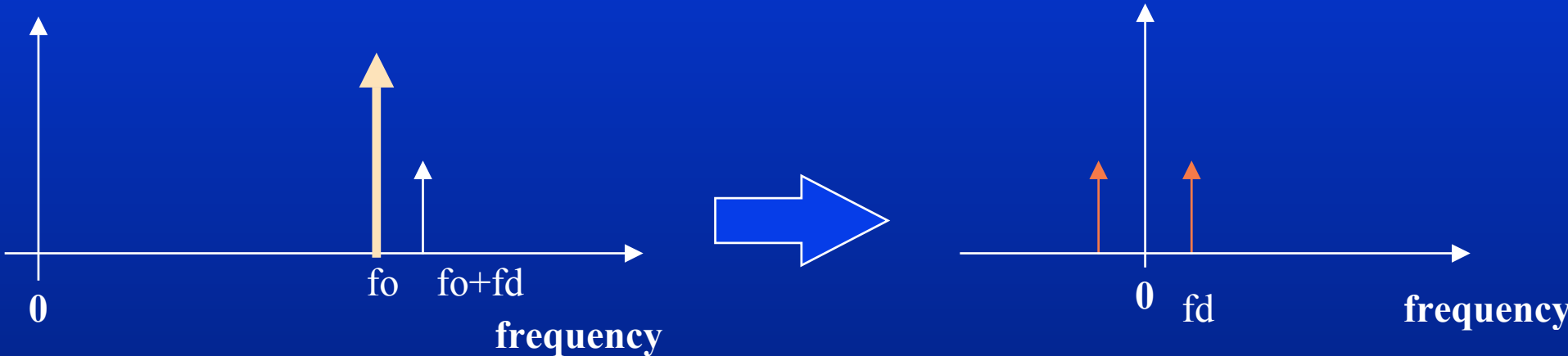


Example : Blood velocity 15 cm/s \sim 0.01 % of 1540 m/s

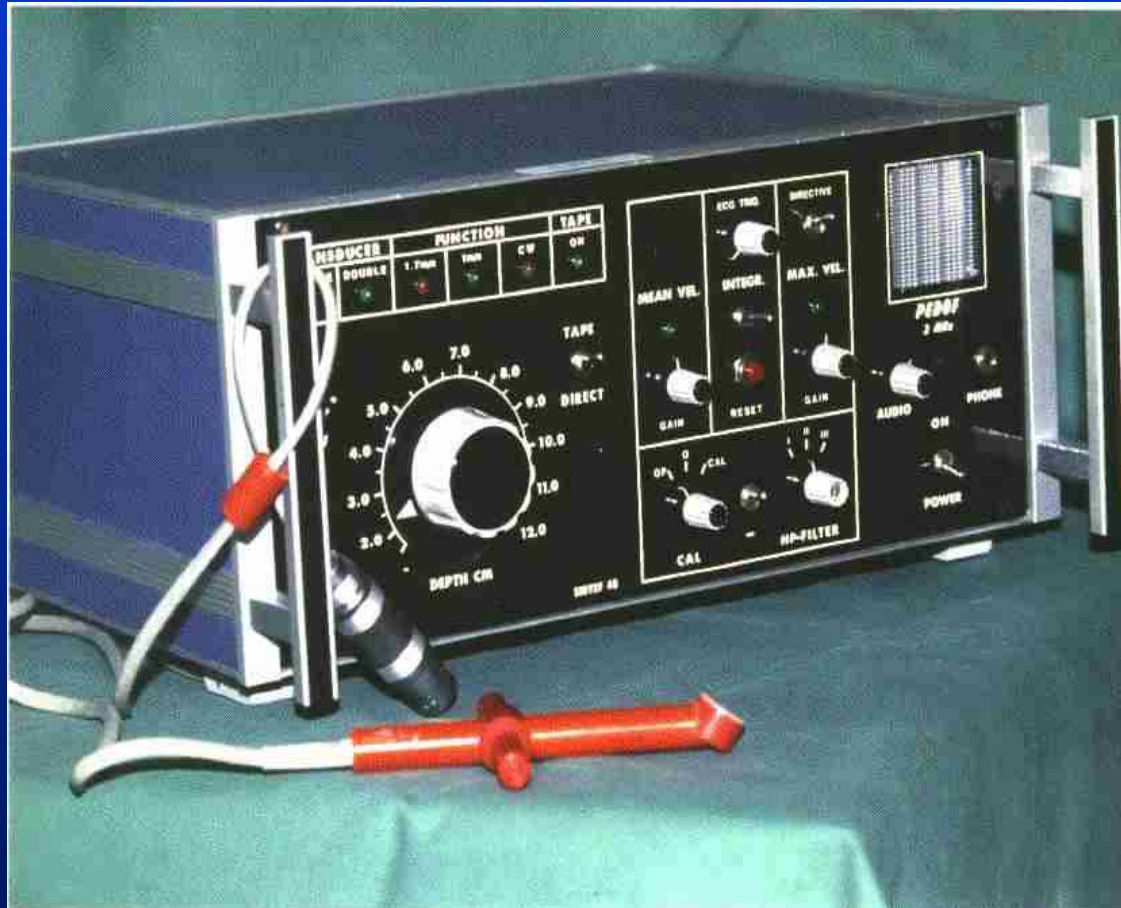
Dopplershift = $2 * 0.01 \% * 5 \text{ MHz} = 1000 \text{ Hz} \sim$ Soprano C

Signal processing for CW Doppler

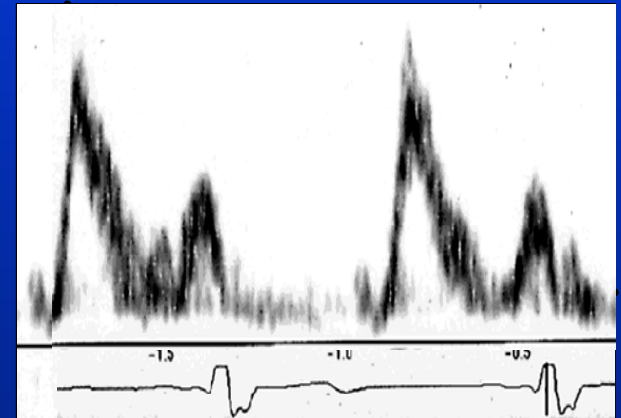
Amplitude detector gives audio Doppler signal



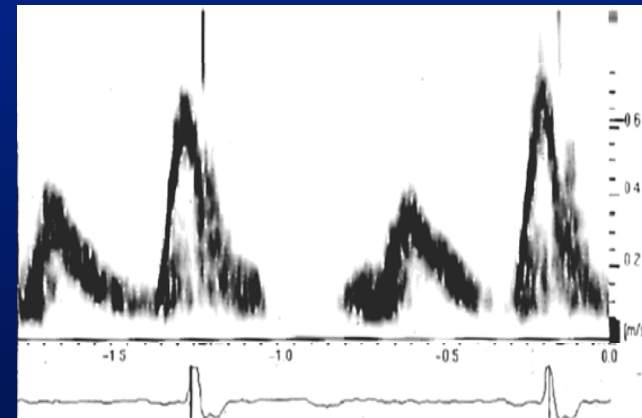
CW/PW Doppler blood flow meter



Blood velocity Mitral inflow

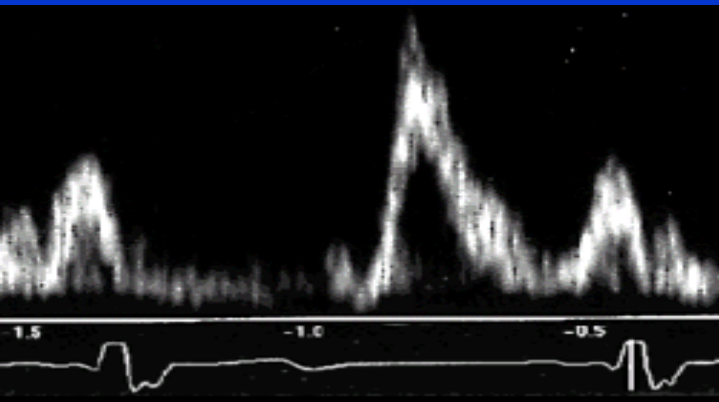


Normal relaxation

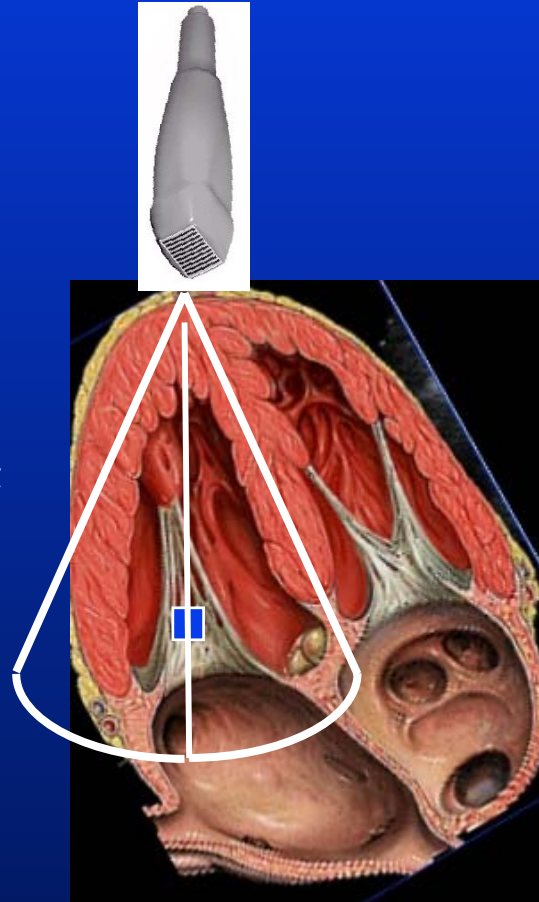


Delayed relaxation

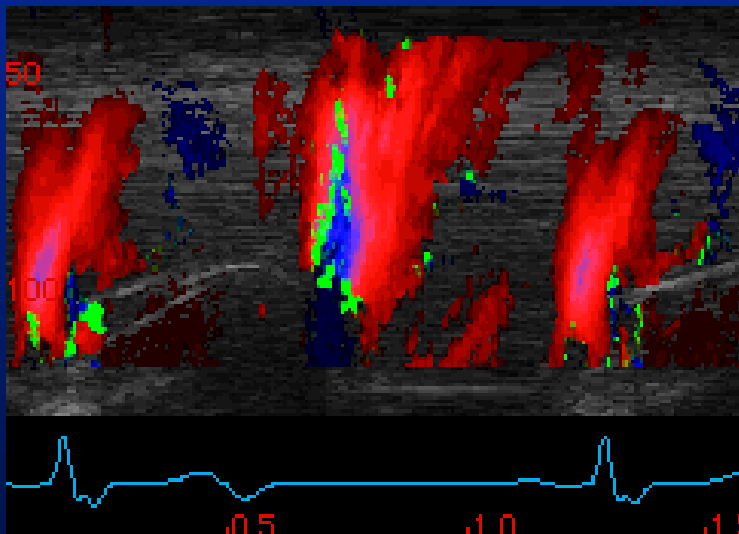
Color Doppler velocity imaging



PW Doppler: Velocity from one point



**Color flow imaging:
Velocities in the whole image**

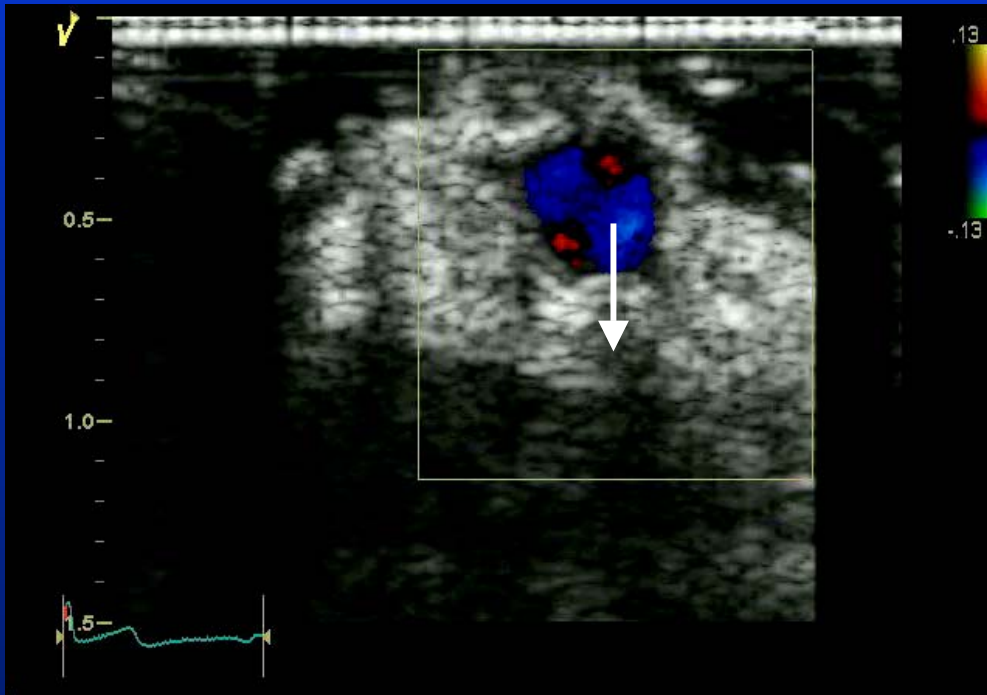


Color M-mode: Velocities along a line

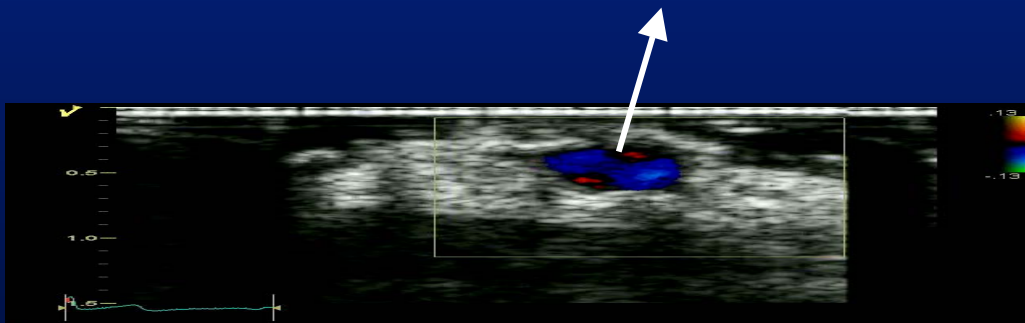


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Flow –integration of normal velocity component over area

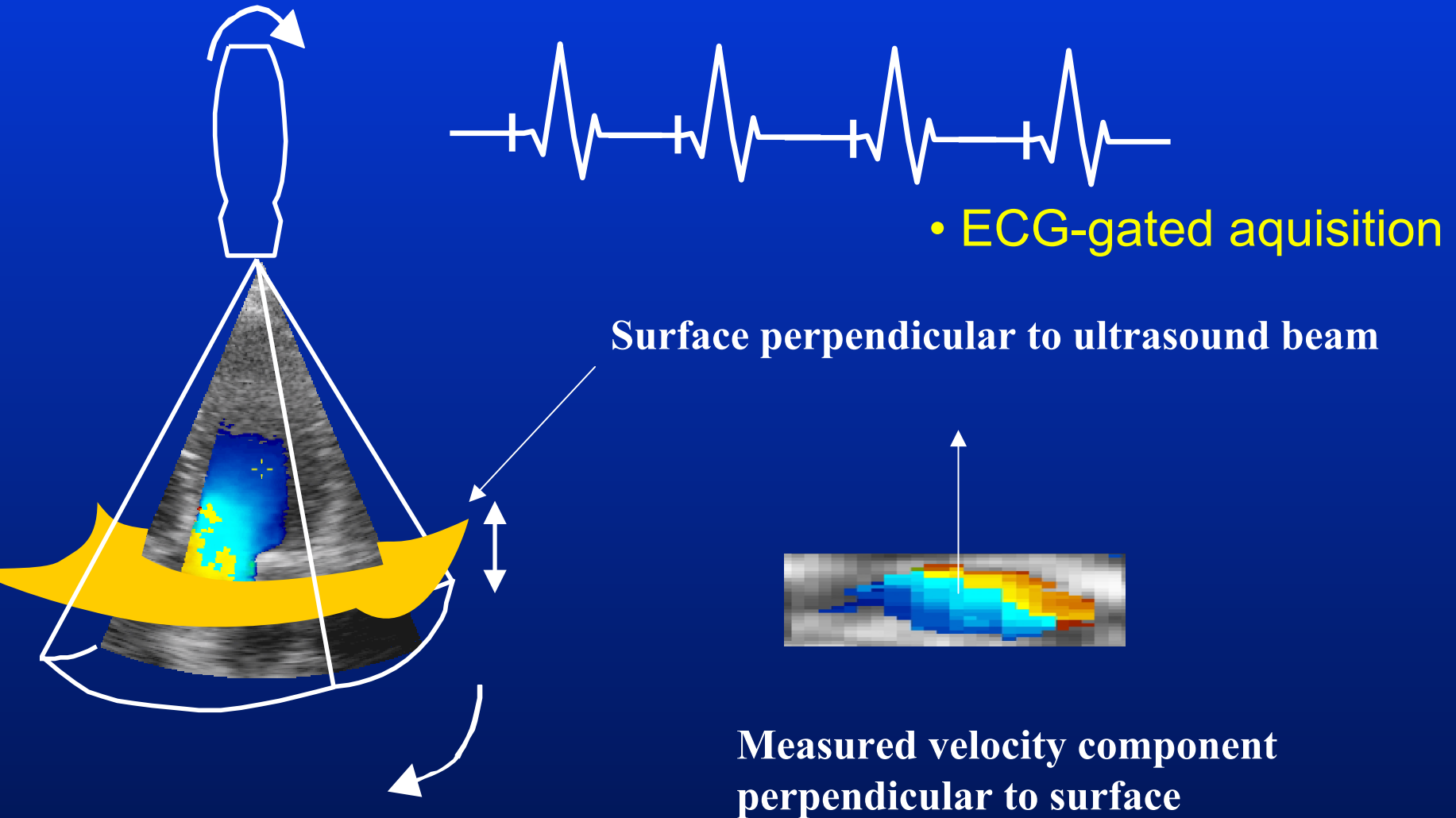


Color flow imaging gives
one velocity component
- along the beam
- in the scan plane



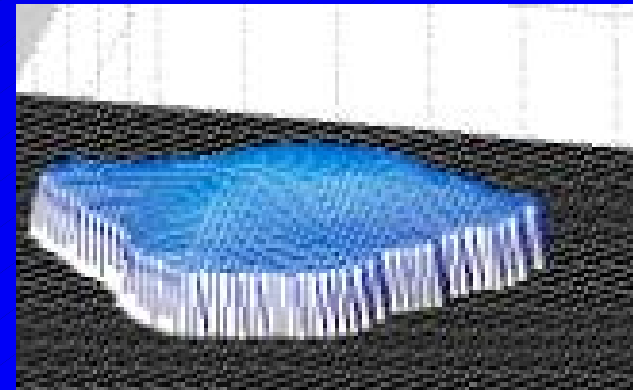
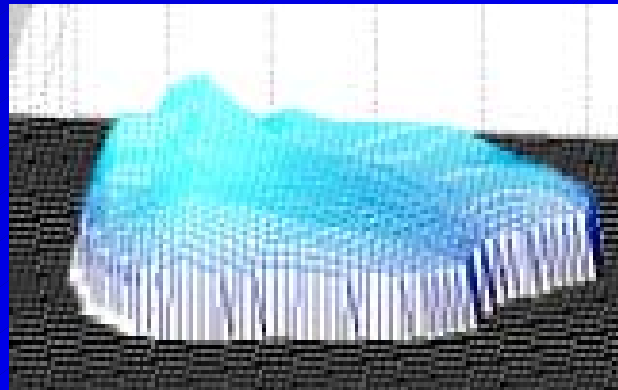
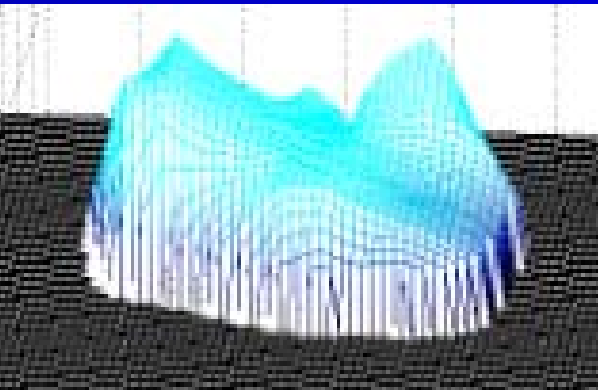
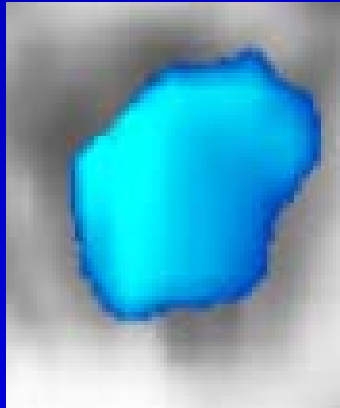
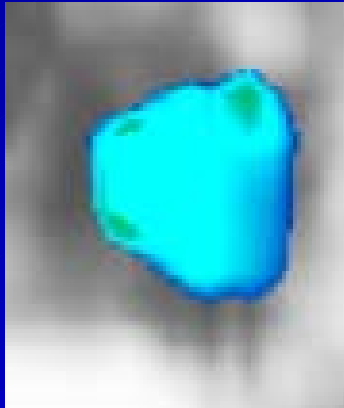
Velocity component
normal to scanplane
is needed for
volume flow calculation

Dynamic 3D Color flow imaging



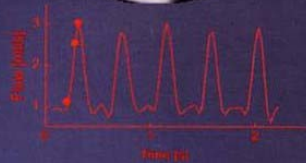
Dynamic 3D Color flow imaging

- Crossectional velocity profiles
- High frame rate (104 frames per second)
- Volume flow obtained by spatial integration



Velocity measurement by decorrelation

Image and Signal Processing in Intravascular Ultrasound



WENGUANG LI

3.3 RESULTS AND COMPARISONS

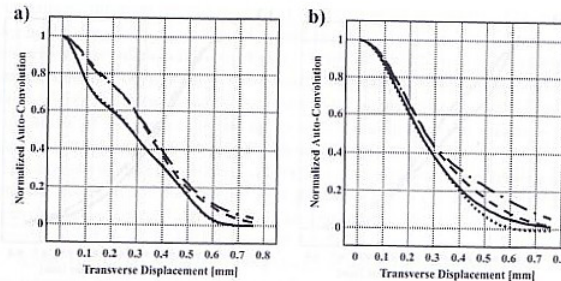


Figure 3.5: Comparison between the Amplitude (A_{1D} (dotted line) and A_{2D} (solid line)) and Energy (E_{1D} (dash-dotted line) and E_{2D} (dashed line)) reference curves. a) Near field (1 mm) and b) Far field (3 mm).

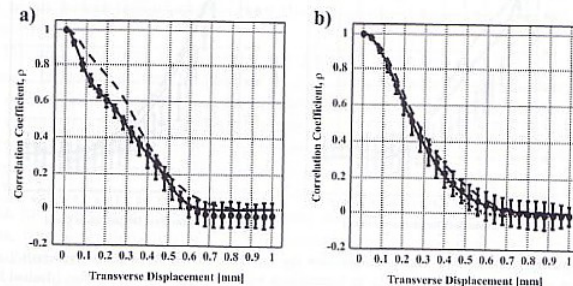


Figure 3.6: Mean decorrelation pattern from RF signals as a function of transverse displacements (error bars); a comparison with three reference curves the A_{1D} (dotted line) and the A_{2D} (solid line) and E_{2D} (dashed line). a) Near field (1 mm) and b) Far field (3 mm).

Quantitative Blood Flow as Assessed by Intravascular Ultrasound

Fermín A. Lupotti

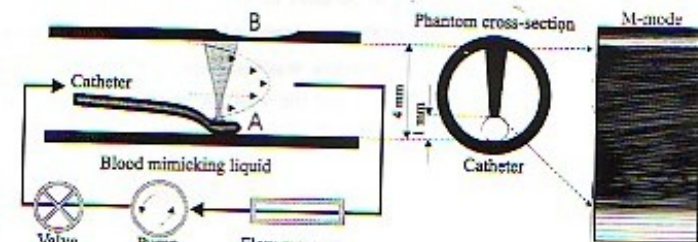
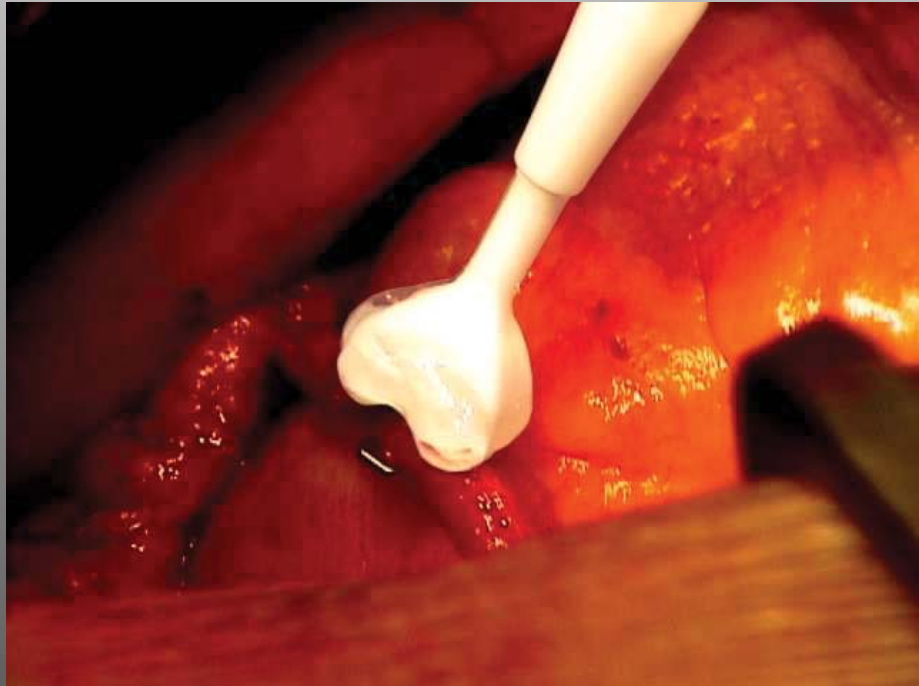


Fig. 5. Illustration of RF data acquisition for in vitro experiment setup. The contrast

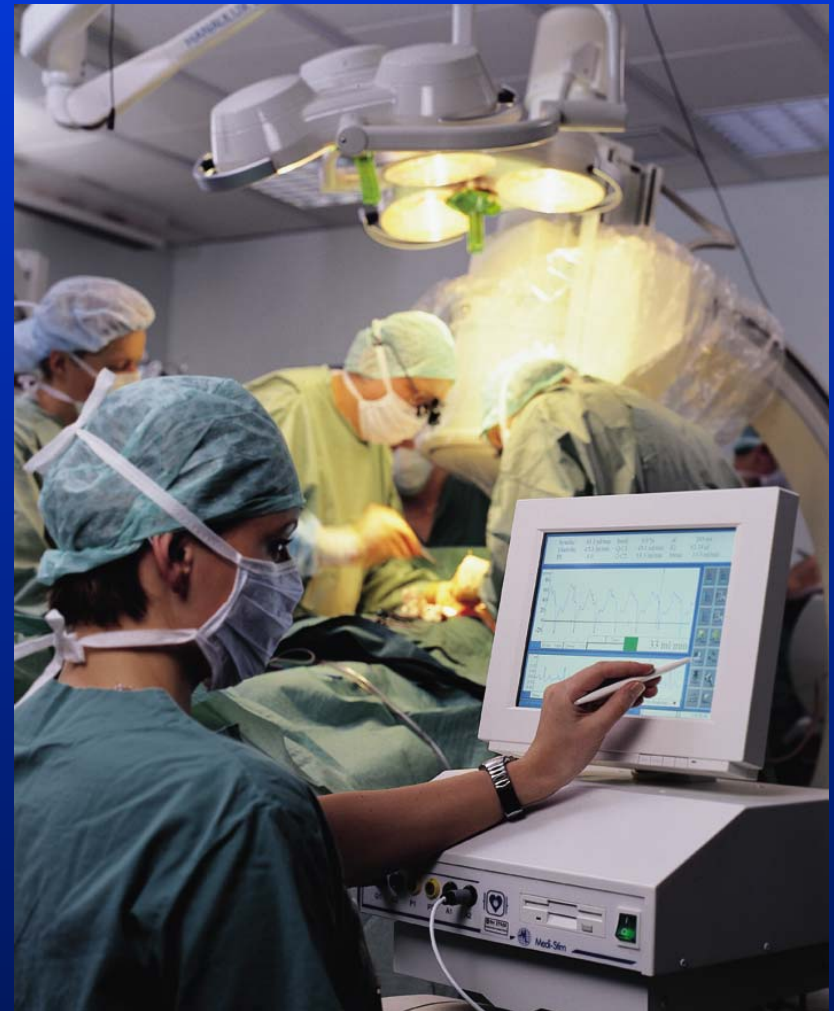
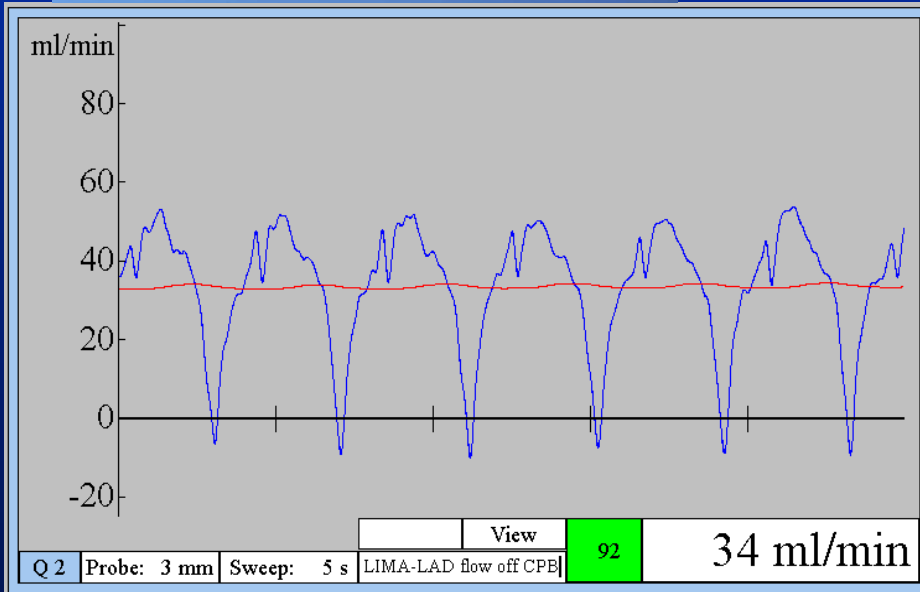
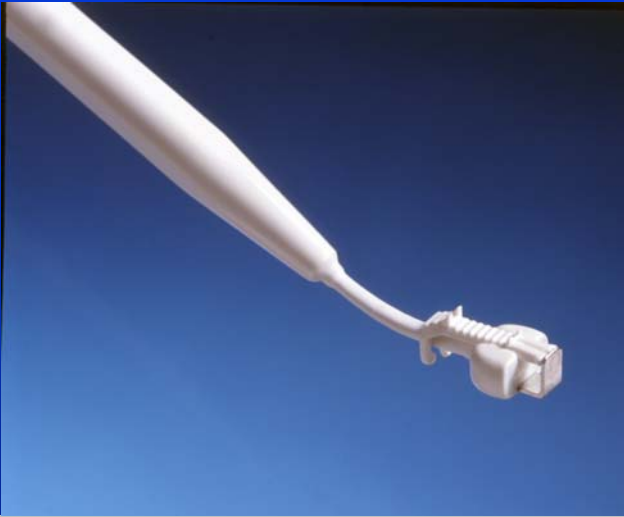
Velocity components normal to scanplane give increased bandwidth ~ decreased correlation
Non-directional technique
Can be integrated to volume flow
Low clutter level required (IVUS)

Ultrasound Transit Time flow-meter

Graft Patency Verification

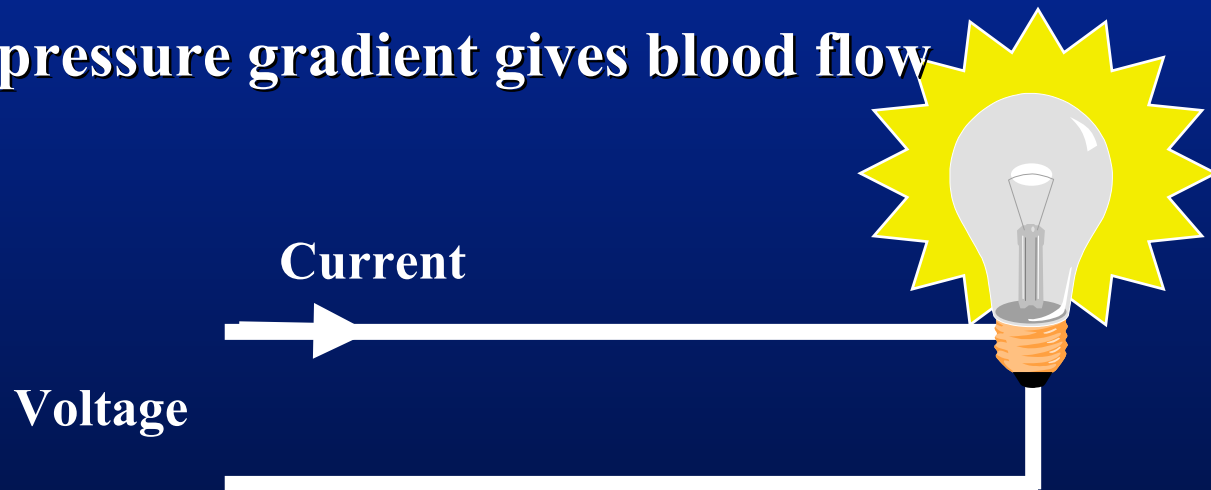


Graft Patency verification

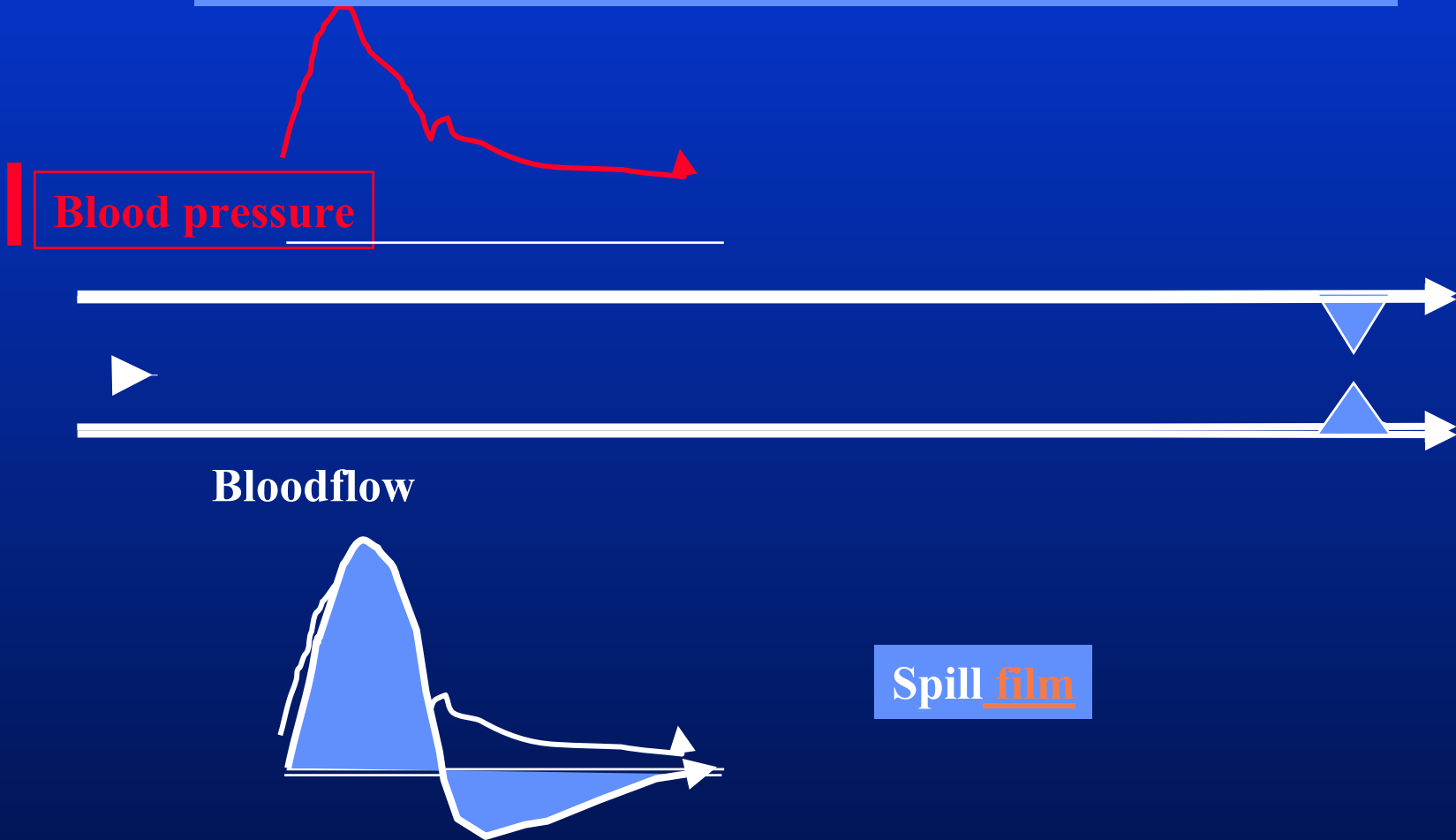


Hemodynamics

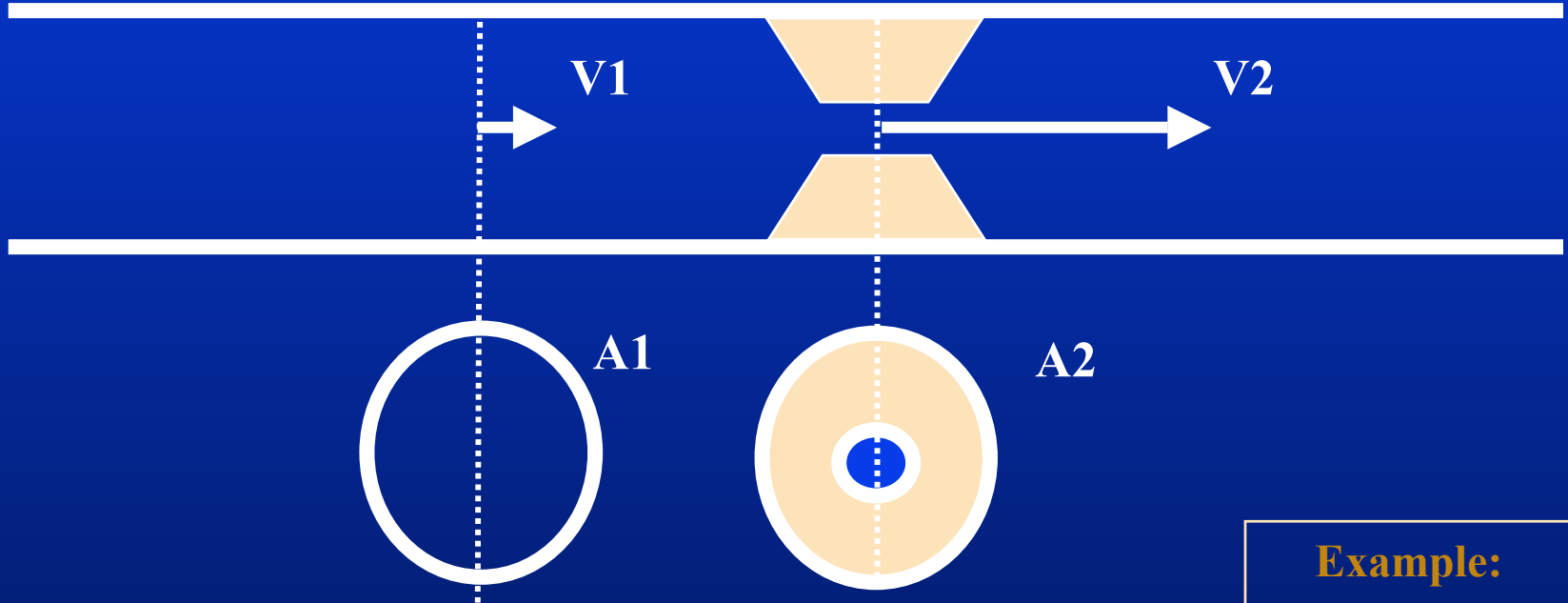
- Hemo from *Haima* = Blood
- Dynamics from *Dynamis* ~ Force which create motion
- Blood pressure gradient gives blood flow



Blood flow, high periferal resistance



Continuity of flow to assess stenosis



$$V1 * A1 = V2 * A2$$

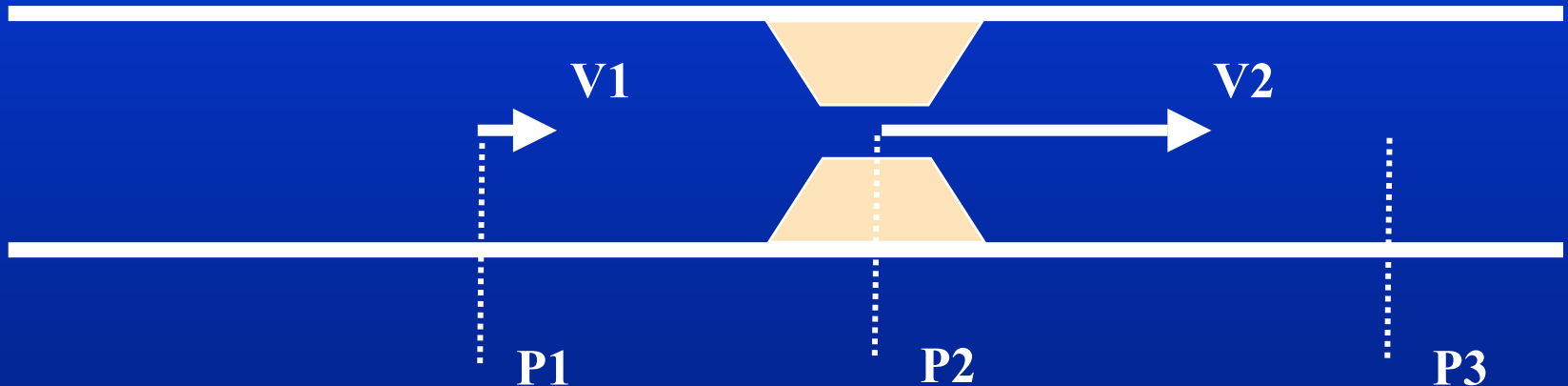
$$\text{\% reduction} = \frac{A1 - A2}{A1} = \frac{V2 - V1}{V2}$$

Example:

**5x velocity
corresponds to
80% stenose**

Area reduction depends only on the velocity $V2/V1$; independent of diameter and angle

Reduction in blood pressure in a stenosis



Pressure drop (gradient) : $P1 - P3 = 4 V2^2$

Example: 80% aortic-stenosis

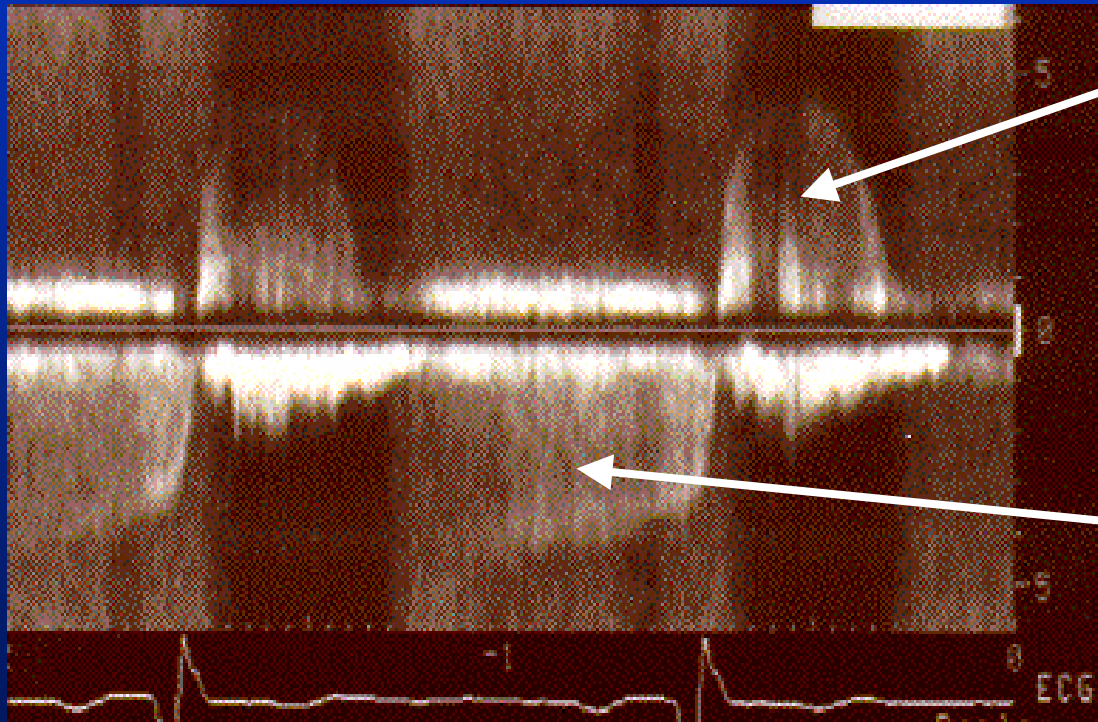
$V1 = 1 \text{ m/s}$ $V2 = 5 \text{ m/s}$ pressure-gradient $4 * 5 * 5 = 100 \text{ mmHg}$

Normal aortic pressure 120 mmHg corresponds to

220 mmHg ventricular pressure!



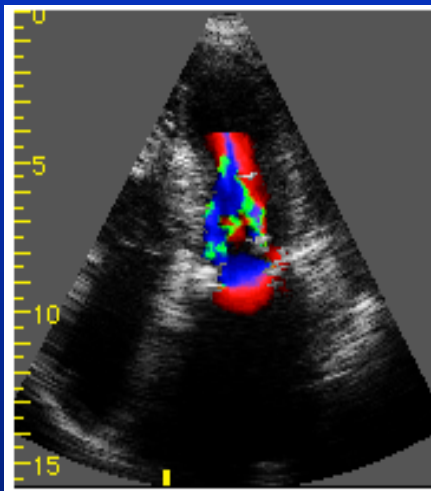
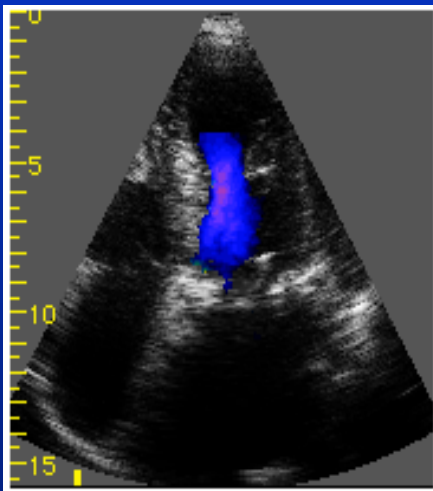
Aortic stenosis + regurgitation by CW Doppler



**Stenosis
(forward flow)**

**Regurgitation
(reverse flow)**

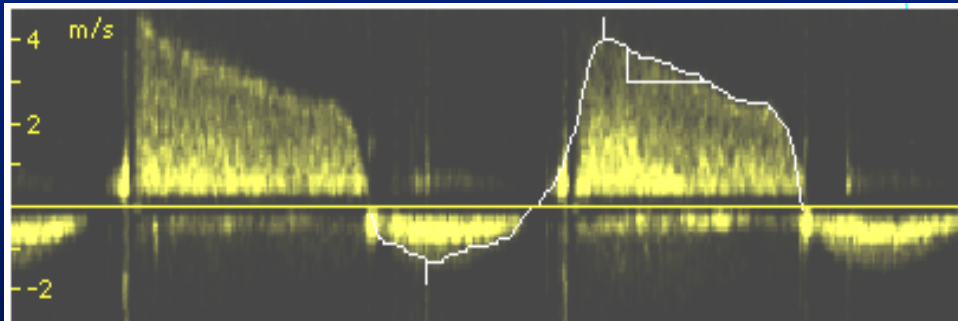
Mitral valve prosthesis with reduced opening area



**Simplified Bernoulli
equation:**

Pressure gradient
 $dP = 4 v^2$

Doppler shift



Time

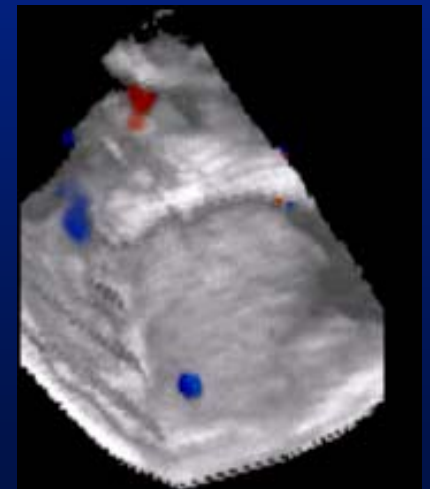
**Pressure half time
decay gives
mitral valve area**

Cardiac dynamic 3D imaging

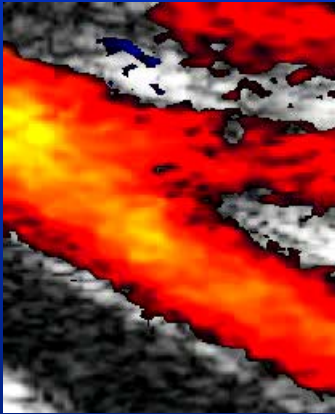


**Magnetic position
sensor system**

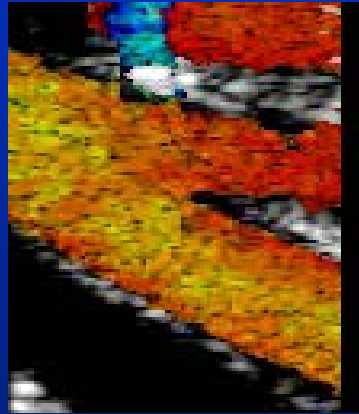
**Mitral valve with lupus
(vegetation) and
reverse flow**



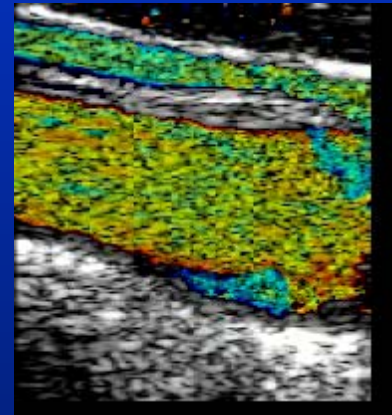
Blood motion imaging: Visualize flow direction in color flow imaging



**Arteria brachialis
Conventional CFI**



**Arteria brachialis
BMI**



**Carotis communis
BMI**



Off-pump bypass surgery

Rune Haaverstad

Stein Samstad

Hans Torp

Vis film!

